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Preparation and oxygen sensing properties of a sol-gel derived thin film based on a covalently grafted ruthenium(II) complex

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Abstract

The preparation and properties of luminescent oxygen sensing materials based on a sol–gel derived thin film containing covalently grafted $Ru(bpy)_3^{2+}$ fragments are described in this article. The 2,2'-bipyridyl covalently grafted to 3-aminopropyltriethoxysilane through Si–CH₂ covalent bonds was used as not only one of the sol–gel precursors but also the second ligand of $Ru(bpy)_2Cl_2\cdot 2H_2O$ complex to prepare the sol–gel derived silicates for oxygen sensors. The luminescence of covalently grafted Ru(II) within the thin film can be extremely quenched by oxygen with good sensitivity ($I_0/I_{100} = 4.3$) and rapid response time (7 s), which suggests that the covalently grafting strategy presented in this article can be used for developing oxygen sensors. Furthermore, the thin film possesses the distinct advantages over those obtained by the physically entrapped method due to the Si–CH₂ covalent bonds, including greatly minimized dye leaching effect, faster detection and simplified linear Stern–Volmer plot. © 2006 Elsevier B.V. All rights reserved.

Keywords: Oxygen sensor; Ruthenium complex; Sol-gel method; Covalent grafting

1. Introduction

Life on earth relies on the presence of oxygen (O_2) and other gases in the atmosphere. The determination of O_2 concentration is important as O₂ is often involved in many chemical and biochemical reactions as reactants or products. Traditionally, O₂ is quantified by using a Clark-type amperometric electrode, which is based on the electroreduction of O_2 on a polarized cathode. In recent years, optical oxygen sensors are more attractive than conventional amperometric devices due to the following advantages: faster response time, high sensitivity and selectivity, no O₂ consumption, no poison and no requirement for a reference electrode [1–10]. The optical oxygen sensors mainly operate on the principle of oxygen quenching of dye molecules, which have been entrapped into a porous support matrix. The ruthenium(II) polypyridyl complexes are one of the most widely used oxygen-sensitive dyes because of their efficient quenching by molecular O2, relatively long fluorescence lifetime determined

by the metal-to-ligand charge-transfer (MLCT) excited state, fast response time, strong visible absorption, large Stokes shift and high photochemical stability [6,7,9,11–18]. The sol-gel approach is an efficient immobilization technique for oxygen sensors based on ruthenium complexes due to its many desirable properties such as high thermal stability, good photostability and optical transparency in the visible light region [7,9,10,19–21]. Unfortunately, there are significant drawbacks when using these systems for oxygen sensors because only weak physical interactions exist between the dopants and the matrix, including inhomogeneous distribution of both organic/inorganic components, leaching of dopants, and poor flexibleness [10,18–20,22]. In order to overcome the above-mentioned drawbacks, here we present a strategy to prepare a novel sol-gel derived oxygen sensing thin film based on covalently grafting the Ru(II) complex to the backbone of silica networks via Si-CH₂ covalent bonds. The luminescent and oxygen-sensing properties were systemically investigated. The typical sensitivity of the obtained film defined by I_0/I_{100} is 4.3 where I_0 and I_{100} denote the fluorescence intensities under 100% nitrogen and 100% oxygen condition, respectively. The response time t_0 and recovery time t_R are 7 and 23 s, respectively, which indicates that the thin film obtained

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in our present work meet the requirements of an oxygen sensor. Detection of dissolved oxygen can be expected because of the greatly improved anti-leaching, sensitivity, and stability of this kind of covalently grafted thin films.

2. Experimental

2.1. Chemical reagents

4,4'-Dimethyl-2,2'-bipyridyl and anhydrous RuCl₃ (99.99%) along with the 3-aminopropyltriethoxysilane (APS) were obtained from Aldrich (Milwaukee, WI, USA) and were used without further purification. Tetraethoxysilane (TEOS) and EtOH were purchased from Tianjin Chemicals Co. Concentrated HCl and thionyl chloride (SOCl₂, A.R.) were obtained from Shanghai Chemical Co. SOCl₂ was used after distillation in vacuo. The complex bis(2,2'-bipyridyl)ruthenium(II) chloride dihydrate, Ru(bpy)₂Cl₂·2H₂O, was synthesized and purified as

described in the literature [23]. The water used in our work is de-ionized.

2.2. Sample preparation

The ligand (denoted as Bpy-Si, as shown in Scheme 1) was prepared using 2,2'-bipyridine-4,4'-dicarboxylic acid and APS as the starting materials. The synthesis of 2,2'-bipyridine-4,4'-dicarboxylic acid was performed by oxidation of 4,4'-dimethyl-2,2'-bipyridine by reflux in a potassium permanganate aqueous solution as described in detail in Ref. [23]. The detailed synthetic procedure of Bpy-Si has been reported elsewhere [24,25] and can be briefed as follows: 2,2'-bipyridine-4,4'-dicarboxylic acid (0.49 g; 2.00 mmol) was dissolved in excess distilled SOCl₂ (8 mL) and refluxed for 4 h. The excess SOCl₂ was eliminated by evaporation from the yellow solution, and the residual was reacted with APS under nitrogen for 4 h at room temperature in the presence of excess pyridine and using

Scheme 1. Synthesis procedure of hydrolysable Ru(bpy)₂(Bpy-Si)Cl₂ complex and the predicted structure of the finally obtained oxygen sensing material.

diethyl ether as a solvent (40 mL). Pyridinium hydrochloride was filtered and evaporation of the residual organic solvent gave the alkoxysilane-modified bipyridine ligand Bpy-Si.

To obtain the hydrolysable complex $Ru(bpy)_2(Bpy-Si)Cl_2$, a mixture of $Ru(bpy)_2Cl_2$ and Bpy-Si in anhydrous ethanol was refluxed for 8 h in nitrogen atmosphere to give a transparent deep red solution, indicating that the complexation reaction between Bpy-Si and $Ru(bpy)_2Cl_2$ had finished. The molar ratio of Bpy-Si to $Ru(bpy)_2Cl_2$ was 1.02:1. Finally the ethanol was rotary evaporated off and the residue was dried in vacuo without any further purification.

The sol-gel derived thin film for an oxygen sensor was prepared using Ru(bpy)2(Bpy-Si)Cl2 as one of the precursor, which reacted with TEOS by hydrolysis and condensation. The following particular procedure was chosen because it is representative of TEOS-based xerogels reported in literatures [6,7,13,19,24–27]. A starting solution was prepared by dissolving the complex Ru(bpy)₂(Bpy-Si)Cl₂ (14.2 mg) in ethanol (1.5 mL) in a plastic vial and stirred for 5 min, and then 5 mL of TEOS was added for another 5 min stirring, followed by H₂O and HCl addition. A minimal amount of tetrahydrofuran was added to the solution to solubilize the Ru(II) complex in the sol more efficiently. The final molar ratio of constituents was TEOS: $H_2O:C_2H_5OH:HCl = 1:4:4:0.01$. The concentration of Ru(bpy)₂(Bpy-Si)Cl₂ in the final sol was 2×10^{-3} M. The solution was kept stirring at room temperature for 4 h prior to the dip-coating of the sol onto a freshly cleaned sodalime silicate glass substrate. Each side of the glass substrate was firstly cleaned by soaking in 1 M NaOH for 30 min and washing 10 times with deionized water and EtOH, finally dried under ambient conditions. The withdrawing rate was set as 5 cm/min to give a wet gel film. The as-synthesized thin film was dried under ambient conditions in the dark for at least 2 weeks before any measurement. Finally, optically transparent crack-free thin film was obtained and the adhesion of the sol to the substrate was found to be excellent.

2.3. Instruments and measurements

The infrared absorption spectra were measured in the region of $400\text{--}4000\,\text{cm}^{-1}$ by a Fourier transform infrared (FTIR) spectrophotometer (Model Perkin-Elmer Model 580B) with a resolution of $\pm 4\,\text{cm}^{-1}$ using the KBr pellet technique. The UV–vis electronic absorption measurements of the final products were performed with a Shimadzu UV-3000 spectrophotometer with a resolution of $\pm 1\,\text{nm}$.

The photoluminescence (PL) spectra of the thin films prepared were obtained in aerated environments by a Hitachi F-4500 fluorescence spectrophotometer equipped with a monochromator (resolution: 0.2 nm) and a 150 W Xe lamp as the excitation source. Suitable filters were used to correct for the baseline shift due to any stray light.

The oxygen sensing properties of our present sol-gel derived thin film were discussed based on the fluorescence intensity quenching instead of the excited state lifetime because it is hard to obtain the precise excited state lifetime value with a conventional flashlamp-based time-correlated photo-counting system. The excitation wavelength of all samples was 475 nm. The excitation spectrum was obtained monitoring at the wavelength of peak emission (625 nm).

For the Stern–Volmer plot measurement, oxygen and nitrogen were mixed at different concentrations via gas flow controllers and passed directly to the sealed gas chamber. We typically allowed 1 min between changes in the N_2/O_2 concentration to ensure that a new equilibrium point had been established. Equilibrium was evident when the luminescence intensity remained constant ($\pm 2\%$). The O_2 concentrations were accurate to $\pm 1\%$ [28]. The sensor response curves were obtained using the same method.

In the measurement of fluorescence lifetime of the Ru complex incorporated within the thin film, a 266 nm light generated from the Fourth-Harmonic-Generator pumped by a pulsed Nd:YAG laser was used as an excitation source. The Nd:YAG laser was with a line width of $1.0\,\mathrm{cm}^{-1}$, pulse duration of 10 ns and repetition frequency of 10 Hz. A Rhodamine 6G dye pumped by the same Nd:YAG laser was used as the frequency-selective excitation source. All measurements were performed at room temperature.

3. Results and discussion

By using the double-role Bpy-Si compound, as a second ligand for complex Ru(bpy)₂Cl₂ and as a sol–gel precursor, we have succeeded in covalently grafting the complex Ru(bpy)₃Cl₂ to the functionalised silicates produced via a sol–gel approach for oxygen sensors. The synthesis procedure of this material is outlined in Scheme 1.

The presence of organic ligands covalently bonded to the network of the modified silicate is characterized by FTIR. The FTIR spectra of hydrolysable Ru(bpy)₂(Bpy-Si)Cl₂ complex (a) and the final oxygen sensing material (b) are shown in Fig. 1. In Fig. 1a, the spectrum of Ru(bpy)₂(Bpy-Si)Cl₂ is dominated by ν (C–Si, 1208 cm⁻¹) and ν (Si–O, 1079 cm⁻¹)

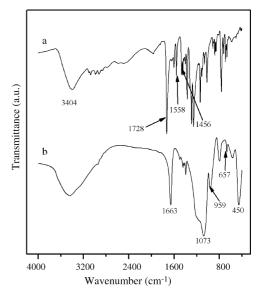


Fig. 1. FTIR spectra of (a) hydrolysable Ru(bpy)₂(Bpy-Si)Cl₂ complex and (b) the finally obtained oxygen sensing material.

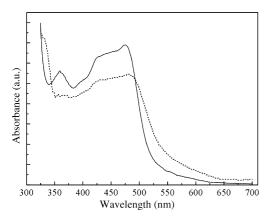


Fig. 2. Optical absorption spectra of Ru(bpy)₂(Bpy-Si)Cl₂ complex in ethanol (solid line) and the final oxygen sensing material (dash line).

absorption bands, which are the characteristics of trialkoxylsilyl functions [29]. Furthermore, the bending vibration of Si-O at 462 cm⁻¹ from APS is obvious in Fig. 1a, indicating that the APS has been successfully grafted onto 2,2'-bipyridine [24]. In panel b of Fig. 1, the formation of the Si-O-Si framework is evidenced by the bands located at 1088 and $1080\,\mathrm{cm}^{-1}$ (ν_{as} , Si-O), 802 and 799 cm⁻¹ (ν_s , Si-O), and 456 and 462 cm⁻¹ (δ , Si–O–Si) (ν represents stretching, δ in-plane bending, s symmetric, and as asymmetric vibrations) [24]. The peaks at 1656 and 1636 cm⁻¹, originating from the CONH group of Bpy-Si, can also be observed in the as-synthesized material, which is consistent with the fact that the Bpy-Si group in the framework remains intact after the hydrolysis/condensation reaction. Furthermore, the broad absorption band at 1120–1000 cm⁻¹ corresponding to the $\nu(\text{Si-O-Si})$, as shown in Fig. 1b, indicates the formation of siloxane network. The introduction of TEOS and water to the Ru(bpy)₂(Bpy-Si)Cl₂ results in the changes in the IR spectra (as shown in Fig. 1a and b) due to the hydrolysis/condensation of TEOS and Ru(bpy)₂(Bpy-Si)Cl₂. The remained ν (Si-C) vibration located at 1208 cm⁻¹ indicates that no (Si-CH₂) bond cleavage occurs during the hydrolysis/condensation reactions.

Fig. 2 represents the optical absorption spectra of $Ru(bpy)_2(Bpy\text{-Si})Cl_2$ complex in ethanol and the final oxygen sensor material. Both absorption spectra show an intense band at 475 nm which can be assigned to the MLCT $(t_{2g}(Ru) \rightarrow \pi^*(L))$ transition, and a smaller band at 360 nm originated from metal centered (MC) d–d transition [30–33]. The shoulder at 427 nm is attributed to the splitting of the first excited state energy level into two separate levels caused by the trigonal symmetry of the complex [31–34]. As shown in Fig. 2, the absorption features of $Ru(bpy)_2(Bpy\text{-Si})Cl_2$ complex entrapped in the final oxygen sensor material are not significantly changed from that observed in ethanol, indicating that there is no interaction between the complex and the sol–gel matrix in the energetically ground state.

Fig. 3 shows the fluorescence emission spectra of Ru(bpy)₂(Bpy-Si)Cl₂ complex dissolved in ethanol and the final thin film oxygen sensor. We can see that the emission spectra show a broad band ranging from 550 to 750 nm. The broadband fluorescence emission arises from ligand to metal charge-transfer excited state where the emitting state is derived from a configuration involving promoting a metal d electron to a ligand

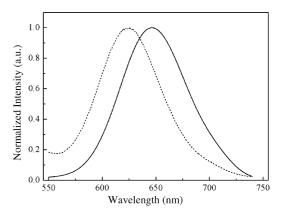


Fig. 3. Emission spectra of Ru(bpy)₂(Bpy-Si)Cl₂ complex dissolved in ethanol (solid line) and the final thin film oxygen sensing material (dash line).

 π^* antibonding orbital [15]. The emission maximum wavelength shows a blue shift of 21 nm from 646 to 625 nm when the complex is immobilized within the sol–gel derived thin film. This is probably caused by the change of the MLCT excited state within the hybrid thin film during the formation of Si–O network structure. Such a blue shift can be explained on the basis of the suppression of the vibrational deactivation and the restriction on the mobility of the Ru(II) complex in an excited-state due to the rigidity of silica matrix [16,18,35–37].

Optical sensors based on the luminescence quenching are examined by the Stern–Volmer equation. In homogeneous media with a single-exponential decay, the intensity and lifetime forms of the Stern–Volmer equation with dynamic quenching are as follows:

$$\frac{I_0}{I} = \frac{\tau_0}{\tau} = 1 + K_{SV}[O_2] = 1 + \kappa \tau_0[O_2]$$
 (1)

where I and τ are the fluorescence intensity and excited-state lifetime of the luminophore, respectively, the subscript 0 denotes the absence of oxygen, $K_{\rm SV}$ is the Stern–Volmer constant, κ is the bimolecular rate constant describing the efficiency of the collisional encounters between the luminophore and the quencher, and $[O_2]$ is the oxygen concentration. A plot of I_0/I or τ_0/τ versus oxygen concentration should give a straight-line relationship with a slope $K_{\rm SV}$, and an intercept of 1 on the y-axis [9].

The luminescence of most Ru(II)-bipyridine complexes could be quenched effectively by molecular oxygen. The room temperature emission spectra, which are recorded for a typical covalently grafted Ru(bpy)₂(Bpy-Si)Cl₂ thin film oxygen sensor under different concentrations of oxygen, are presented in Fig. 4. The position and shape of the 625 nm MLCT emission from Ru(bpy)₂(Bpy-Si)Cl₂ is constant under different oxygen concentrations. However, the relative intensity decreases markedly with increasing the oxygen concentration. The relative luminescent intensities of the Ru(bpy)₂(Bpy-Si)Cl₂-doped thin film oxygen sensor decrease by 77.9% upon changing from pure nitrogen to pure oxygen.

Fig. 5 presents the Stern–Volmer plot for a typical covalently grafted $Ru(bpy)_2(Bpy-Si)Cl_2$ thin film oxygen sensor. The estimated uncertainties on the I_0/I are 1–4% based on the precision of the individual intensity measurements. For com-

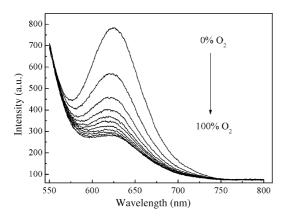


Fig. 4. Emission spectra of a typical covalently grafted Ru(bpy)₂(Bpy-Si)Cl₂ thin film oxygen sensor subjected to different oxygen concentrations.

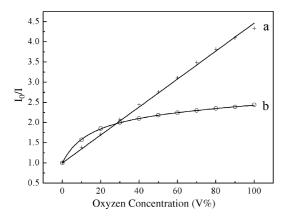


Fig. 5. Typical fluorescence intensity-based Stern–Volmer plots for the oxygen sensors: (a) covalently grafted Ru(bpy)₂(Bpy-Si)Cl₂ thin film and (b) physically incorporated Ru(bpy)₃Cl₂ thin film. The solid lines represent the best fit to a Demas model (the physically incorporated sample, plot b) or Stern–Volmer model (plot a).

parative purpose, the Stern–Volmer plot of an oxygen sensor, in which Ru(bpy)₃Cl₂ was physically incorporated into the sol–gel derived matrix by a conventional method, is also given in Fig. 5. As shown in Fig. 5, the Stern–Volmer plot of the covalently grafted sample shows good linearity; however, the physically incorporated sample without Si–CH₂ covalent bonds exhibits obvious downward curvature. We attribute the good linear Stern–Volmer plot of the covalently grafted sample to the Si–CH₂ covalent bonds that act as a contributor to the network of the modified silicate matrix resulting in the uniform distribution of luminophore. The non-linearity of the physically incorpo-

rated sample is associated with the luminophore molecules being distributed simultaneously between two or more sites within the sol–gel derived silicate in which one site is more heavily quenched than the other [15,38–40]. Consequently, the different microheterogenous sites exhibit different quenching constants $K_{\rm SV}$ and unquenched lifetime τ_0 values. In this case, the single-exponential decay Stern–Volmer equation (as shown in Eq. (1)) cannot be used to describe the oxygen sensing data. In this kind of microheterogenous solid-based oxygen sensor, a two-site model has been found to have excellent ability to fit the experiment data [7,9,22]. In this model, the straight-line intensity-based Stern–Volmer equation then becomes.

$$\frac{I_0}{I} = \frac{1}{\frac{f_{01}}{1 + K_{SV_1}[O_2]} + \frac{f_{02}}{1 + K_{SV_2}[O_2]}}$$
(2)

where f_{0i} valuables are the fraction of each of the two sites contributing to the unquenched intensities and the K_{SVi} values are the associated Stern–Volmer quenching constants for the two sites. The fitting parameters of Fig. 5 are tabulated in Table 1.

For oxygen sensors, short response and recovery time are very important when exposed to practical application. Generally, 95% response time, i.e., $t\downarrow$ (95%, $N_2 \rightarrow O_2$), is defined as the time required for the luminescent intensity to decrease by 95% on changing from 100% N₂ to 100% O₂. Similarly, 95% recovery time, i.e., $t \uparrow (95\%, O_2 \rightarrow N_2)$, means the time required for the luminescence intensity to reach the 95% of its initial value recorded under 100% N₂ on changing from 100% O₂ to 100% N₂ [5]. Fig. 6 shows the typical dynamic response of the covalently grafted thin film oxygen sensor upon repeated exposure to oxygen/nitrogen cycles in the gas phase. Upon changing to pure O₂, the emission intensity drops very quickly, while upon changing to pure N_2 , the emission intensity increases and recovers to its initial value. From this time dependent measurement we can see that the sensor response is stable and reversible. The evaluated time for the change in the PL signal to 95% of the final value is found to be about 23 s on going from 100% O₂ to 100% N₂ and about 7 s on going from 100% N₂ to 100% O₂. This result shows that the response time is shorter than the recover time distinctly, similar to the results obtained for Pt-OEP in a polymer medium [41], and this difference can be explained by the stronger adsorption of oxygen than that of nitrogen on the silica surface [18].

Fig. 7 shows the typical excited-state intensity decay profile for a randomly selected covalently grafted Ru(bpy)₂(Bpy-Si)Cl₂ thin film measured in the ambient atmosphere. It is clear

Table 1 Intensity-based Stern–Volmer oxygen quenching fitting parameters for covalently grafted $Ru(bpy)_2(Bpy-Si)Cl_2$ thin film and physically incorporated $Ru(bpy)_3Cl_2$ thin film^a

Samples	I_0/I_{100}	Stern-Volmer		Demas ^b			
		$\overline{K_{\rm SV}([{\rm O}_2]^{-1})}$	r^2	$K_{SV1} ([O_2]^{-1})$	K_{SV2} ([O ₂] ⁻¹)	f ₀₁ ^c	r^2
Physically incorporated thin film Covalently grafted thin film	2.44 4. 29	0.0347 (±0.0003)	0.9975	0.1660 (±0.0055) 0.0407 (±0.0017)	$0.0010 (\pm 0.0001)$ $0.0047 (\pm 0.0005)$	0.59 (±0.01) 0.94 (±0.01)	0.9998 0.9999

^a When an entry is not listed, the given model is the best given; Sample aged for 2 months.

^b Terms are from Eq. (2).

 $^{^{}c} f_{01} + f_{02} = 1.$

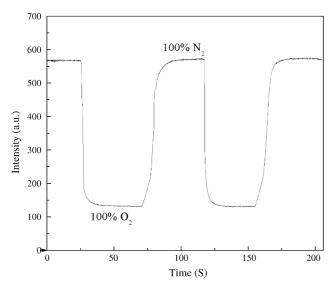


Fig. 6. Relative luminescence intensity of 625 nm emission as a function of time for a typical covalently grafted $Ru(bpy)_2(Bpy-Si)Cl_2$ thin film subjected to an atmosphere which was varied periodically between 100% N_2 and 100% O_2 .

that the final thin film luminescence exhibits an almost single exponential excited-state decay profile, confirming the fact that Ru(II) complex molecules within the modified silicate occupy the same microenvironment sites and the distribution is uniform and homogeneous. These results are similar to that previously reported by Bright et al. [7]. The result of the excited-state intensity decay profile is consistent with the Stern–Volmer plot (as shown in Fig. 5).

Dissolved oxygen sensing is of major importance in environmental, industrial and medical applications. One fundamental but crucial question that remains when this kind of covalently grafted oxygen sensor is used for the dissolved oxygen detection is whether the luminophore leaches into the liquid phase. For this consideration, complex-leaching experiment was performed by soaking the covalently grafted Ru(bpy)₂(Bpy-Si)Cl₂ thin film in water, DMF and ethanol at 60 °C in a sealed cuvette under magnetic stirring and then dried at 100 °C in vacuo, as described previously [27]. These results reveal that the covalently grafted oxygen sensor possesses greatly enhanced chemical durability in

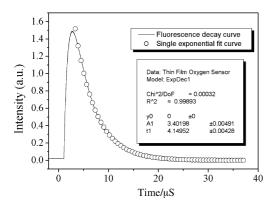


Fig. 7. Typical excited-state intensity decay profile for a randomly selected covalently grafted Ru(bpy)₂(Bpy-Si)Cl₂ thin film. The scatter line is the best fit to the experimental data using the single exponential decay model.

comparison with the physically incorporated thin film. The integrated fluorescence intensities of the unquenched MLCT emission of the covalently grafted sample after stirring in each solvent for 5 days were stable and no leaching effect was observed, while the integrated fluorescence of the physically incorporated sample dropped by 45%. This result reveals that the Si–CH₂ covalent bonds between the complex and the sol–gel matrix can effectively prevent the dopant leaching, which entirely agrees with the report by Li et al. [27]. The great minimization of the leaching is a crucial aspect for the dissolved oxygen sensor applications. Work is currently underway in our laboratory to fully characterize the dissolved oxygen sensing properties.

4. Conclusion

A covalent grafting strategy about preparation of optical sol-gel derived thin films for oxygen sensor material with high photochemical stability and good linearity Stern-Volmer plot was presented in this article. No leaching effect can be observed since these luminescence molecules were covalently grafted to the Si-O network; this properties make them show potential applications in monitoring the dissolved oxygen in liquid phase. The Si-CH₂ covalent bonds between the Ru(II) complex and the sol-gel derived modified silicate matrix as a network contributor result in enhanced anti-leaching, sensitivity, homogeneous distribution and linearity of the Stern-Volmer plot. This new kind of covalently grafted thin film can be further improved via changing the microstructure of the sensor support, and further work is in progress. Furthermore, the covalent grafting strategy reported in this article allows one to extend this method to prepare other organometallic complex doped devices with high performance.

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