## Highly sensitive oxygen sensors based on Cu(I) complex–polystyrene composite nanofibrous membranes prepared by electrospinning<sup>†</sup>

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The first optical oxygen sensor based on Cu(1) complexpolystyrene composite nanofibrous membranes, showing high sensitivity  $(I_0/I_{100} = 15.56)$ , good linear Stern-Volmer characteristics ( $R^2 = 0.9966$ ) and short response/recovery time  $(t_{\downarrow} (s) = 7 \text{ and } t_{\uparrow} (s) = 14)$ , has been prepared; these results represent the best values reported for oxygen sensors based on Cu(1) complexes.

Over the past decades, the development of oxygen sensors has been extensively pushed because the determination of molecular oxygen content in gas and liquid phases is very important in many different fields, such as oceanography, meteorology, biology, environmental science and life science.<sup>1</sup> Commonly, optical oxygen sensors are based on noble metal complexes, *e.g.*, Pt(II), Ru(II), Au(I), Ir(III) and Re(I) complexes.<sup>2</sup> However, their wide utilization is largely limited due to their extremely high cost. Recently, luminescent Cu(I) complexes have attracted great attention owing to their highly emissive metal-to-ligand-charge-transfer (MLCT) state, long luminescence lifetimes, large Stokes shift and low cost. Nevertheless, few oxygen sensors based on Cu(I) complexes have been reported.<sup>3</sup>

For optical oxygen sensing devices, it is necessary to incorporate the luminescent complexes into a solid matrix, such as sol–gel-derived silica-based materials,<sup>4</sup> mesoporous silicas<sup>5</sup> and polymers.<sup>6</sup> Recently, nanofibers prepared by electrospinning have been proved to be excellent host materials for developing functional materials because of their large surface area-to-volume ratio, the unique nanoscale architecture, and the simple and cost-effective preparation method.<sup>7</sup> Electrospun nanofibrous membranes have approximately one to two orders of magnitude more surface area than that found in continuous thin films.<sup>7d</sup> It is expected that the large amount of available surface area of electrospun nanofibrous

membranes is helpful to improve oxygen sensor performances. However, up to now, there has been no report on oxygen sensors based on polymer nanofibers by electrospinning as the matrix.

In this contribution,  $[Cu(POP)phencarz]BF_4$  (POP = bis[2-(diphenylphosphino)phenyl]ether; phencarz 2-(Nethyl-carbazole-yl-4)imidazo[4,5-f]1,10-phenanthroline) was incorporated into polystyrene (PS) matrices, and electrospun into composite nanofibrous membranes. The optical oxygen sensing properties of [Cu(POP)phencarz]BF<sub>4</sub>-PS composite nanofibrous membranes were investigated. High sensitivity  $(I_0/I_{100} = 15.56)$ , good linear Stern–Volmer characteristics  $(R^2 = 0.9966)$  and short response/recovery time  $(t_{\perp} (s) = 7)$ and  $t_{\uparrow}$  (s) = 14) were obtained. A performance comparison shown in Table 1 between this work and literature values suggests that [Cu(POP)phencarz]BF<sub>4</sub>-PS composite nanofibrous membranes represent the best oxygen sensing performances reported for oxygen sensors based on Cu(I) complexes. Phencarz and  $[Cu(POP)phencarz]BF_4$  were prepared according to literature methods<sup>8</sup> and the structure of [Cu(POP)phencarz]BF<sub>4</sub> is depicted in Fig. 1 (I). The typical procedure for electrospinning composite nanofibers can be found in the ESI.<sup>†</sup> In the following text, [Cu(POP)phencarz]-BF<sub>4</sub>-PS composite nanofibrous membranes electrospun from 1, 1.5, 2 and 3 wt% concentrations relative to PS in N,N-dimethylformamide solution are labelled as samples A, B, C and D, respectively.

The scanning electron microscope (SEM) image and fluorescence microscopy image of sample B are shown in Fig. 1. It is observed that the obtained electrospun nanofibers are smooth, uniform, and evenly distributed on the substrate with a random orientation. The diameter for the composite fibers is 500–700 nm. The fluorescence photography of sample B shows bright green emission of [Cu(POP)phencarz]BF<sub>4</sub> arising from the MLCT excited state, suggesting that

**Table 1** Representative examples of reported  $I_0/I_{100}$  values of opticaloxygen sensors based on Cu( $\mathfrak{l}$ ) complexes

Sensor materials	$I_0/I_{100}$	Linear relationship	Ref.
[Cu(POP)phencarz]BF <sub>4</sub> –PS	15.56	Near-linear	This work
$[Cu(dbp)(dmp)](PF_6)-PS$	1.70	Near-linear	3 <i>a</i>
[Cu(POP)(PTZ)]BF <sub>4</sub> -MCM-41	11.16	Non-linear	3 <i>b</i>
[Cu(dpephos)(pip)]BF <sub>4</sub> -SBA-15	7.44	Non-linear	3 <i>c</i>
[Cu(dpephos)(epip)]BF <sub>4</sub> -SBA-15	5.68	Non-linear	3 <i>c</i>
[Cu(dpephos)(nip)]BF <sub>4</sub> -SBA-15	5.51	Non-linear	3 <i>c</i>
[Cu(dpephos)(enip)]BF <sub>4</sub> -MCM-41	5.95	Non-linear	3 <i>c</i>

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**Fig. 1** (I) The molecular structure of [Cu(POP)phencarz]BF<sub>4</sub>; (a) scanning electron microscope (SEM) image and (b) fluorescence microscopy image of sample B.

 $[Cu(POP)phencarz]BF_4$  was successfully electrospun into composite nanofibrous membranes.

UV-vis absorption spectra of [Cu(POP)phencarz]BF<sub>4</sub>, PS and sample B are given in Fig. S1 of the ESI.† As for [Cu(POP)phencarz]BF<sub>4</sub>, the absorption bands located around 260, 290 and 330 nm are attributed to spin-allowed ligandcentered transitions. The absorption band from 360 to 480 nm is experimentally assigned to MLCT [ $d\pi$ (Cu) $-\pi$ \*(phencarz)] transition compared with the absorption spectra of POP and phencarz (see ESI, Fig. S2†).<sup>3b</sup> Two absorption bands exist, located around 258 and 309 nm in pure PS fibers. All the absorption bands aforesaid are found in the spectrum of sample B, confirming that [Cu(POP)phencarz]BF<sub>4</sub> is successfully incorporated into PS matrices.

In order to test the oxygen sensing performances of  $[Cu(POP)phencarz]BF_4-PS$  composite nanofibrous membranes, emission spectra of samples A, B, C and D were recorded under different oxygen concentrations at room temperature (see ESI, Fig. S3†) and that of sample B is presented in Fig. 2. The emission peaks centered at about 510 nm originate from MLCT transition. Upon excitation by light in a pure nitrogen atmosphere, the Cu(1) complex transitions from the ground state to a higher energy state (excited state), and when returning



**Fig. 2** Emission spectra of sample B under different oxygen concentrations. Inset: Stern–Volmer plot for sample B under different oxygen concentrations.  $\lambda_{ex} = 365$  nm.

to ground state, it emits light. As oxygen molecules enter, bimolecular collisions between the excited Cu(I) complex molecules and the ground state (triplet) oxygen relax the luminophore nonradiatively, resulting in singlet oxygen (excited state). Thus, a quenching process occurs. The corresponding sensing mechanism can be described as:

$$Cu(I)^* + O_2 \rightarrow Cu(I) + O_2^*$$

where Cu(1) denotes the [Cu(POP)phencarz]BF<sub>4</sub> molecule and "\*" is the excited state. The relative luminescence intensities of samples A, B, C and D decrease by 92.6, 93.0, 92.0 and 90.9%, respectively, upon changing from pure nitrogen to pure oxygen. Sample B (1.5 wt%) is not only more sensitive compared with other samples, but also shows the strongest emission intensity. We speculate that the reason for this is as follows: when the doping concentration is low (1 wt%), emission from the probe is comparatively weak, which results in the low sensitivity; when it is too high (2 and 3 wt%), aggregation between probe molecules may become serious, resulting in low emission intensity. As a result, 1.5 wt% [Cu(POP)phencarz]BF<sub>4</sub> relative to PS is the optimum level.

Oxygen quenching is diffusion-limited and can be described by the Stern–Volmer relationship<sup>9</sup> in the simplest scenario of a luminophore in a homogeneous microenvironment:

$$I_0/I = 1 + K_{\rm SV}[O_2] = 1 + k_q \tau_0[O_2]$$

where *I* is the steady-state luminescence intensity of luminophore, the subscript 0 denotes the absence of oxygen,  $\tau_0$  is the excited-state luminescence lifetime in the absence of oxygen,  $K_{SV}$  is the Stern–Volmer constant,  $k_q$  is the bimolecular rate constant describing the efficiency of the collisional encounters between the luminophore and the quencher, and [O<sub>2</sub>] is the oxygen concentration. For this ideal case, a plot of  $I_0/I vs.$  [O<sub>2</sub>] will be linear with a slope equal to  $K_{SV}$  and an intercept of unity, allowing a simple single-point sensor calibration. The lifetime decay of the luminophore in homogeneous media can be described by a single-exponential equation:<sup>10</sup>

$$I(t) = \alpha \exp(-t/\tau)$$

where I(t) is the luminescence intensity at time *t*, and  $\alpha$  is the pre-exponential factor.

The Stern–Volmer plot of sample B exhibits good linearity  $(R^2 = 0.9966)$  over the full oxygen concentration range studied (0-100% O<sub>2</sub>) as shown in Fig. 2, suggesting that all [Cu(POP)phencarz]BF<sub>4</sub> molecules are in very similar microenvironments within the composite nanofibrous membranes. Nonlinear Stern-Volmer plots arise when luminophores are distributed simultaneously between two or more sites, in which one site is more heavily quenched than the other. Consequently, the microheterogenous sites exhibit different quenching constants  $K_{SV}$  and unquenched lifetime  $\tau_0$  values. Fig. 3 presents the time-resolved intensity-decay curve of sample B in the absence of oxygen (pure  $N_2$ ). A single exponential decay law best described the observed intensity decay, which is consistent with the Stern-Volmer plot shown in Fig. 2. All these data confirm that [Cu(POP)phencarz]BF4 molecules are distributed homogeneously within the composite nanofibrous



Fig. 3 Time-resolved intensity-decay curve of sample B in the absence of oxygen (pure  $N_2$ ). The fit to a single-exponential decay model is shown (solid line).

Table 2Oxygen-sensing properties of the  $[Cu(POP)phencarz]BF_4-PS$ composite nanofibrous membranes and the PS thin films with 1.5 wt% $[Cu(POP)phencarz]BF_4$  prepared by different methods

А	В	С	D
14.38 0.1394	15.56 0.1492	13.46 0.1312	11.62 0.1138
Spin coati	ng <sup>a</sup> Dip	Dip coating <sup>a</sup>	
5.82 0.2606 0.0005	7.8 0.2 0.0	7.84 0.2543 0.0006	
	A 14.38 0.1394 Spin coatin 5.82 0.2606 0.0005	A         B           14.38         15.56           0.1394         0.1492           Spin coating <sup>a</sup> Dig           5.82         7.8           0.2606         0.2           0.0005         0.00	A         B         C $14.38$ $15.56$ $13.46$ $0.1394$ $0.1492$ $0.1312$ Spin coating <sup>a</sup> Dip coating <sup>a</sup> $5.82$ $7.84$ $0.26066$ $0.2543$ $0.0005$ $0.0006$

<sup>*a*</sup> Demas "two-site" model is used to fitting the PS thin films with 1.5 wt% [Cu(POP)phencarz]BF<sub>4</sub> prepared by different methods.

membranes. The oxygen sensing properties of all samples are summarized in Table 2. A sensor with  $I_0/I_{100}$  more than 3.0 is a suitable oxygen sensing device.<sup>2a</sup> The value of  $I_0/I_{100}$  of sample B achieves 15.56, and this is by far the highest value for optical oxygen sensors based on luminescent non-noble metal complexes. For comparison, the PS continuous thin films with 1.5 wt% [Cu(POP)phencarz]BF<sub>4</sub> are prepared by spin coating, dip coating and casting, respectively. Inspection of these data shows that the sensitivity  $(I_0/I_{100})$  ranges from 5.53 to 7.84, indicating that the oxygen sensing performances of the electrospun nanofibrous membranes are superior to those of continuous thin films. We attribute these results to three factors. Firstly, the excited-state lifetime of [Cu(POP)phencarz]BF<sub>4</sub>–PS nanofibrous membrane is quite long (up to 110 µs), offering enough time for bimolecular collision between [Cu(POP)phencarz]BF4 and oxygen molecules. Correspondingly, the [Cu(POP)phencarz]BF<sub>4</sub> lifetimes in thin films and in solution are less than 10 µs (see ESI, Table S2<sup>†</sup>). Secondly, PS is an excellent host material since it is oxygen permeable. Last, but most important, the porous structure of the electrospun membranes not only provides a large surface area-to-volume ratio, but also facilitates the oxygen entry and diffusion.<sup>11</sup> At the same time, we obtain the shortest recovery time for oxygen sensors based on luminescent Cu(I) complexes (see the ESI<sup>+</sup>). We ascribe the fast response/recovery to the fact that the porous structure of the electrospun membranes facilitates the high diffusion of oxygen. The obtained oxygen-sensing performances of [Cu(POP)phencarz]BF4-PS nanofibrous membranes indicate that they are superior to the commonly used Clark-type electrode in some aspects, *e.g.*, the stability of signals, response time, interferences and cost.

In summary, composite nanofibrous membranes as optical oxygen sensors based on low-cost Cu(1) complexes were successfully prepared by electrospinning, exhibiting the highest sensitivity among optical oxygen sensors based on Cu(I) complexes, near-linear Stern-Volmer characteristics, and short response/recovery time. The excellent performances can be explained by the fact that the porous structure of the electrospun membranes with large surface area-to-volume favors the oxygen diffusion, the PS is an outstanding host material owing to its good oxygen permeating ability, and the excited-state lifetime of [Cu(POP)phencarz]BF<sub>4</sub>-PS composite nanofibrous membranes is long enough for bimolecular collision between [Cu(POP)phencarz]BF4 and oxygen molecules. The outstanding performances, the simple and versatile preparation method, and economical attraction endow this kind of composite nanofibrous membrane with the potential for commercial application in oxygen sensors.

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## Notes and references

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